Three-dimensional ultrasound as a predictor of pregnancy in patients undergoing ART

ART uygulanan hastalarda gebeliği öngörmeye yarayan bir araç olarak üç boyutlu ultrason

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Abstract

Different ultrasound parameters have been used to assess endometrial receptivity during ART treatment, including endometrial thickness, endometrial pattern, endometrial volume, Doppler of uterine arteries and endometrial blood flow. However, conflicting results have been reported with regard to their role in the prediction of pregnancy in ART treatment. The 3D ultrasound with power Doppler provides a unique tool with which to examine the blood supply of the whole endometrium and subendometrial region. Volume assessment can also be precisely performed by 3D ultrasound. Based on a med-line research and on our experience, the clinical use of 3D ultrasound is discussed in this review article.

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Introduction

Three-dimensional ultrasound (3D-US) is a rapidly developing area of clinical imaging. The ongoing research and continuous improvements in 3D-US have a significant impact on many areas of clinical application (1-6).

Successful implantation depends on the interaction between the blastocyst and the endometrium. Thickness of endometrium and a good blood supply are considered to favour pregnancy (7-9). Increased endometrial and subendometrial vascularity have been found to be higher in patients with live births following Assisted Reproductive Technology (ART) than in those who have suffered a miscarriage (10). However, conflicting results are reported with regard to their role in the prediction of pregnancy in ART treatment (11-13).

We developed this review through the use of Medline, a digital database, articles on three-dimensional ultrasonography and pregnancy outcomes in patients undergoing ART. In addition, we used the data we collected over the past 12 years and our clinical experiences.

Özet

ART tedavisi sırasında endometriyumun kabul ediciliğini değerlendirmek için farklı ultrason parametreleri kullanılmaktadır. Bunlar içinde endometriyal kalınlık, endometriyal patern, endometriyal hacim, uterus arterlerinin ve endometriyal kan akımının Doppler'i yer almaktadır. Bununla beraber, ART tedavisinde gebeliğin öngörülmesindeki rolleri ile ilgili olarak birbiriyle çelişen sonuçlar bildirilmiştir. Bütün endometriyumun ve subendometriyal bölgenin kan akımının incelenmesinin mümkün olduğu power Doppler'li 3D ultrason yegane bir araç sağlamaktadır. 3D ultrason ile hacim değerlendirmeleri de kesin olarak yapılabilmektedir. Med-line araştırması ve kendi deneyimimize dayanarak, bu derleme makalede 3D ultrasonun klinik kullanımı tartışılmaktadır. (J Turkish-German Gynecol Assoc 2012; 13: 128-34) **Anahtar kelimeler:** 3D, ultrason, power Doppler, IVF, ART

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Volume calculation

Volume calculation by 3D-US will be performed by Virtual Organ Computer-Aided Analysis (VOCAL) program. VOCAL is the combination of 3D ultrasound tissue presented as voxels and geometric information of surfaces in a 3D dataset. It is defined by rotating an image plane around a fixed axis and defining 2D contours of each plane. The 2D contours of the polygonal area in each plane can be defined automatically or manually. There are four rotation angles to choose from: 6° , 9° , 15° and 30° , and because the entire dataset is rotated about 180,° these result in 30, 20, 12 and 6 planes, respectively, being available for measurements. The result is converted to mL or cm³ ultrasound units (Figure 1).

In a previous study we documented the reproducibility of the endometrial volume measurement in 57 consecutive patients undergoing in-vitro fertilization (14). The interobserver reliability was 0.96 with an intraobserver reliability of 0.94. High reproducibility was also obtained for ovarian volume and power Doppler indices (15-19).

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Figure 1. 3D-volume calculation in a VOCAL program. Note the 2D contours of the endometrium have to be defined in different planes



Figure 2. Differences of estimated volumes and real volumes (vertical axis) are plotted against the real volumes (horizontal axis). For a better view, the single points of each method (2D, 3D, first, second measurement) were connected by lines

We evaluated the in-vivo accuracy of 3D volume measurements of the uterus (20). In this study, transvaginal ultrasound examinations were performed in 48 consecutive patients before hysterectomy. Immediately after hysterectomy, the true volume was measured in a water bath. Although the volumes estimated by the 3D method were not significantly different (p=0.126), the volumes estimated by the 2D method were significantly different (p=0.005). The mean error rate of the 3D volume measurement was 7.4%, and 22.2% for the 2D volume measurement (Figure 2, Table 1). The limitation of the uterine volume measurement by 3D was the uterine size. An uterus more than 220 ml. could not be measured accurately. The high accuracy of volume measurements by 3D ultrasound was also confirmed by other studies (21-25).

Volume storing

Although 2D ultrasound makes it possible for physicians to make important contributions to patient management, there are occasions when it is difficult to develop a 3D impression of the patient's anatomy. The typical approach to overcome this problem is to scan repeatedly through the region-of-

	Number	Minimum	Median	Maximum	Mean	Standard- deviation	Variance
2D Vol 1	35	31.2	113.7	274.2	121.6	69.8	4871.2
2D Vol 2	35	28.8	114.0	299.3	120.5	70.2	4931.9
3D Vol 1	35	36.2	102.7	237.6	111.8	61.0	3719.1
3D Vol 2	35	35.4	104.5	241.6	108.5	56.5	3192.8
Real Volume	35	35	100	220	109	57	3199
Vol3D1-Vol*	35	-20.10	3.40	44.30	2.98	11.35	128.74
Vol3D2-Vol*	35	-21.10	-1.50	51.60	34	12.37	153.09
Vol2D1-Vol*	35	-47.60	15.50	84.20	12.79	27.26	743.15
Vol2D2-Vol*	35	-45.80	14.00	109.30	11.65	28.03	785.45
ABS(Vol3D1-Vol)**	35	.20	6.40	44.30	8.20	8.29	68.68
ABS(Vol3D2-Vol)**	35	1.10	6.90	51.60	8.46	8.92	79.48
ABS(Vol2D1-Vol)**	35	3.20	16.90	84.20	23.98	17.88	319.63
ABS(Vol2D2-Vol)**	35	5.20	17.40	109.30	23.20	19.26	370.99
*Difference of estimated volume-real volume, **Absolute difference of estimated volume-real volume							

Table 1. Shows that the median of the absolute differences for 3D (estimated volume-real volume) lies between 6.4 and 6.9, whilst for 2D the median lies between 16.9 and 17.4

interest (ROI) to make an exact diagnosis. This process can be time consuming and tedious. Furthermore, time consuming examinations can alienate the patients. In contrast to 2D ultrasound, which allows particular planes, 3D volume acquisition enables the presenting of the whole organ simply, so that the whole organ can be stored for later examinations. In addition, this ability has an important "teaching effect" as it allows a re-evaluation of the examination after histologic findings of tumors and such.

3D-power Doppler

Quantitative 3D power Doppler angiography represents the acquisition and measurement of power Doppler data within a 3D data set. This technique is being used to compare pregnant and non-pregnant patients undergoing ART. The majority of these studies use the 'histogram' tool, which displays the distribution of the power Doppler data and uses specific algorithms to derive indices of blood flow: vascularisation index (VI) characterises vessel density: the ratio of the number of colour voxels to the total number, flow index (FI) describes the intensity of blood flow: the ratio of the sum of colour intensities to the colour voxels and the vascularisation flow index (VFI) assesses both vascularisation and perfusion: the ratio of the sum of colour intensities to the total number of voxels (Figure 3).

These vascular indices depend on, and relate to, the total and relative amounts of power Doppler information within the target organ and the intensity of the signals. The power Doppler signal is dependent on the presence of blood flow within the target organ and its intensity is dependent on the number of blood cells within the blood vessels. The intensity of the power Doppler spectrum is determined by several settings: gain, pulse repetition frequency (PRF), line density, wall motion filter, signal rise and persistence and speed of acquisition.

Limitations and artifacts

Understanding of how artifacts occur, and what can be done to detect and correct for them, is important in order to avoid mistaking them for a pathology and to make correct interpretations of clinical 3D ultrasound.

Three types of artifacts can be caused by different sources in 3D ultrasound imaging. Some artifacts occur due to the 2D imaging process. Other artifacts are unique to 3D ultrasound, arising from patient motion or rendering method, which alter the appearance of the anatomy. Lastly, there are artifacts that arise as the result of operator choice in selecting which part of the volume to display (26). Each of these artifact sources may alter the displayed images and lead to incorrect diagnosis. Consequently, differentiation of the endometrial border from neighboring structures (e.g. myometrium), may be very difficult, especially in obese women. As a result, volume measurements cannot be performed accurately. In cases where power Doppler signal artifacts exist, power Doppler indices of target organ cannot be measured accurately.

Using power Doppler, it is essential to maintain identical settings if different subjects, or if changes over time within the same subject, are to be compared. One of the most important Doppler settings is color gain. Doppler gain appears to be directly correlated with all the 3D power Doppler indices, and the use of higher gains may lead to false signals that could be interpreted as real blood flow (Figure 4a, b).

Raine-Fenning et al. (27) evaluated how different settings affect the Doppler signal in terms of its quantification by these three indices within a 3D dataset. They found that the gain and signal power have the greatest effect on the power Doppler signal, followed closely by the PRF. The other settings and speed of acquisition also influence the signal, but to a much lesser degree. It is essential to maintain constant Doppler settings if any meaningful comparisons are to be made within and between subjects.



Figure 3. Vascularisation index (VI), flow index (FI) and the vascularisation flow index (VFI) assessed both vascularisation and perfusion



Figure 4. a) Vascularisation of ovarian cyst with low gain. b) Vascularisation of the same ovarian cyst with high gain. Note high grade artifacts

Standardizing the color gain between different machines is almost impossible, as the parameters used to define it differ widely among different companies and on different scales within the same company (28).

Endometrial receptivity

Endometrial receptivity is an important factor in human reproduction. It has usually been assessed by endometrial biopsy. However, such an invasive method is not acceptable when evaluating endometrial receptivity. Ideally, it should be evaluated by a non-invasive method.

Lee et al. (29) first reported endometrial volume changes during spontaneous menstrual cycles assessed by 3D US. These authors performed a longitudinal study on 18 nullipara regularly menstruating women, at 3-6 day intervals during a single menstrual cycle, measuring the endometrial and uterine volume and calculating the "uterus-endometrium" ratio. The mean endometrial volume was 1.23 cm³ (SD: 0.98), ranging from 0.25 cm³ to 5.5 cm³. They found that this ratio decreased throughout the menstrual cycle, reaching a nadir around the 20th day of the cycle, reflecting that endometrial volume was highest at mid luteal phase.

Raine-Fenning et al. (30) analysed the endometrial volume longitudinally in a series of 30 fertile women, having regular menstrual cycles. They found a steady increase of the endometrial volume throughout the follicular phase until ovulation occurs and then remained relatively constant throughout the luteal phase. These findings would be in agreement with histological data in which endometrial growth is restricted to the follicular phase of the menstrual cycle when expansion of the stratum functionalis of the endometrium occurs. This in turn is directly related to the increase of serum estradiol levels. In this study, endometrial volume was found to be greater in parous women. Two parameters are considered to predict pregnancy: a) endometrial volume and b) (sub) endometrial flow.

a) The first studies reported a good correlation between endometrial volume and pregnancy (31-33). Although it has been shown that the endometrium must attain at least 2.0-2.5 ml to achieve a pregnancy, recent studies did not confirm the relation between endometrial volume and pregnancy outcome (33-37). In our study, the area under the receiver operating characteristic (ROC) curve was statistically significant for endometrial volume when no grade 1 embryos or only one were transferred but not significant when two or three grade 1 embryos were transferred (34).

In conclusion, endometrial volume is also unlikely to be predictive of pregnancy, although the pregnancy rate may be significantly reduced in patients whose endometrial volume is less than 2.0-2.5 ml. The suggestion that endometrial thickness is determined by the individual uterine architecture, and therefore not predictive of the likelihood of implantation, may be related to endometrial volume (38).

b) A good blood supply to the endometrium is usually considered as an essential requirement for implantation. Therefore endometrial and subendometrial blood flows were evaluated in several studies. The first study was reported by Schild et al. (39), who measured the subendometrial blood flow on the first day of ovarian stimulation in 75 infertile patients after pituitary down-regulation was confirmed, i.e. endometrial thickness <5 mm, no ovarian cyst of >2.5 cm and serum estradiol concentrations of <60 pg/ml. Subendometrial VI, FI and VFI were significantly lower in pregnant cycles than non-pregnant ones. Logistic regression analysis found that the subendometrial FI was the strongest predictive factor for the outcome among the tested 3D Doppler flow indices.

A recent study by Kim et al. (40) evaluated whether endometrial and subendometrial blood flow parameters measured using three-dimensional power Doppler ultrasound (3D PD-US) can predict pregnancy after intrauterine insemination (IUI). They diagnosed higher endometrium VI, FI, and VFI scores in the pregnant group than in the non-pregnant group. In contrast, the subendometrial region VI, FI, and VFI scores did not differ between the groups. Pregnancies did not occur when endometrial blood flow had not been detected. Therefore, they concluded that three-dimensional PD-US was useful for evaluating endometrial and subendometrial neovascularization in IUI cycles. Similar results were reported by other authors (41, 42).

Ng et al. (43) evaluated endometrial and subendometrial blood flows on the days of human chorionic gonadotrophin (HCG) administration and embryo transfer. They also assessed the percentage change in endometrial and subendometrial blood flows between these two days as a predictor of pregnancy during IVF treatment. A 3D ultrasound examination with power Doppler was performed in 293 patients undergoing the first IVF cycle to determine endometrial thickness, endometrial volume, vascularization index, flow index and vascularization flow index of endometrial and subendometrial regions on the days of HCG administration and embryo transfer. Patients in non-pregnant and pregnant groups had comparable endometrial thickness, endometrial volume and 3D power Doppler flow indices of endometrial and subendometrial regions measured on each day. Percentage changes in endometrial and subendometrial 3D power Doppler flow indices were also similar. In conclusion, endometrial and subendometrial blood flows on the days of HCG treatment and embryo transfer and the percentage change in endometrial and subendometrial blood flows between these 2 days were not predictive of pregnancy.

Vlaisavljević et al. (44) examined whether we might predict the outcome of unstimulated IVF/ICSI cycles with quantitative indices of perifollicular blood flow assessed with three-dimensional power Doppler images. This prospective study included an analysis of 52 unstimulated cycles. Color and power Doppler ultrasound examinations of a single dominant preovulatory follicle were performed on the day of oocyte pick-up. They hypothesized that the follicles containing oocytes able to produce a pregnancy have a distinctive and more uniform perifollicular vascular network.

Conclusion

3D Ultrasound has been proposed as a promising tool for evaluating the endometrium, but a review of the literature regarding its role for assessing endometrial function did not confirm the suggested benefits of this technique. Endometrial volume, endometrial and subendometrial flows have been shown to be ineffective for predicting pregnancy. Interactions between blastocyst and endometrium, e.g. embryo quality, seem to play a more important role than endometrial volume or (sub) endometrial blood flow.

Variable machine settings, differences in examination timing, different Doppler parameters or determination of endometrial volume by uterine architecture may explain why 3D is not predictive in the assessment of pregnancy in patients undergoing ART.

Conflict of interest

No conflict of interest was declared by the authors.

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